I. AMENDMENTS TO THE CLAIMS

Please amend claims 18, 32, 46, 49, 51, 53, 58, 62 and 77, and cancel claims 22, 50 and 66. Please note that the other pending claims, and previously withdrawn claims, have not been revised but are reprinted below for the Examiner's convenience. (The claims have been amended in the manner required by 37 C.F.R. §1.121, as revised 30 July 2003.)

1-17. (Previously Canceled)

- 18. (Amended) A coil for use with a magnetic resonance imaging (MRI) system to form images of a region of a patient [interest] during an MRI scanning procedure, said coil comprising:
- (a) a first ring at one end of said coil, said first ring being electrically conductive and having a first diameter;
- (b) a second ring at an other end of said coil, said second ring being electrically conductive and having a second diameter different from said first diameter of said first ring; and
- (c) a plurality of rods electrically interconnecting said first and said second rings to form said coil therewith, each of said rods having a linear portion and a tapered portion with said linear portion being connected to said first ring and said tapered portion being connected to said second ring, said tapered portions of said rods [collectively providing] configured to provide said coil with a substantially homogeneous pattern of magnetic flux density in at least one of an XZ imaging plane and a YZ imaging plane [three orthogonal imaging planes] of said coil.
- 19. (Previously Presented) The coil claimed in claim 18 wherein said coil is a birdcage coil.
- 20. (Previously Presented) The coil claimed in claim 18 wherein said second diameter of said second ring is smaller than said first diameter of said first ring.
- 21. (Previously Presented) The coil claimed in claim 18 wherein said tapered portion of each of said rods comprises at least one angled linear segmented section.

22. (Canceled)

- 23. (Previously Presented) The coil claimed in claim 18 wherein said first ring and said second ring are each larger in diameter than a center of said coil to thereby enable a concentration of said magnetic flux density to be produced at a region centered within said coil.
- 24. (Previously Presented) The coil claimed in claim 18 further comprising at least one additional coil at least partially overlapping said coil at an inferior end thereof to form therewith, and for operation as, a phased array.
- 25. (Previously Presented) The coil claimed in claim 18 wherein said first and said second rings are circular.
- 26. (Previously Presented) The coil claimed in claim 18 wherein said first and said second rings are elliptical with said first diameter being a major diameter of said first ring and said second diameter being a major diameter of said second ring.
- 27. (Previously Presented) The coil claimed in claim 18 wherein said coil is a receive-only coil.
- 28. (Previously Presented) The coil claimed in claim 18 wherein said coil is a transmit/receive coil.

29. (Previously Presented) The coil claimed in claim 18 wherein each of said rods and said

first and said second rings contain therein a plurality of reactive electrical components.

30. (Previously Presented) The coil claimed in claim 18 wherein said coil is configured as

one of a low pass coil, a high pass coil and a band pass coil.

31. (Previously Presented) The coil claimed in claim 18 wherein said coil is operable in

one of a linear mode and a quadrature mode.

32. (Amended) A coil for use with a magnetic resonance imaging (MRI) system to form

images of a region of a patient [interest] during an MRI scanning procedure, said coil comprising:

(a) a first ring at one end of said coil, said first ring being electrically conductive and

having a first diameter;

(b) a second ring at an other end of said coil, said second ring being electrically conductive

and having a second diameter; and

(c) a plurality of rods electrically interconnecting said first and said second rings to form

said coil therewith, each of said rods having a linear portion and at each end thereof [having] a tapered

portion to which said first and said second rings respectively connect, said tapered portions being

selected to provide said coil with a subsantially homogeneous [maximize homogeneity] pattern of

magnetic flux density in at least one of an XZ imaging plane and a YZ imaging plane of said coil.

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33. (Previously Presented) The coil claimed in claim 32 wherein said first and said second

diameters of said first and said second rings, respectively, are equal.

34. (Previously Presented) The coil claimed in claim 32 wherein said first and said second

diameters are each larger than a diameter at a center of said coil such that said tapered portions of said

rods are tapered outwardly.

35. (Previously Presented) The coil claimed in claim 32 wherein said first and said second

diameters are each smaller than a diameter at a center of said coil such that said tapered portions of

said rods are tapered inwardly.

36. (Previously Presented) The coil claimed in claim 32 wherein said coil is a birdcage

coil.

37. (Withdrawn) A method of designing a coil capable of exhibiting a substantially

homogeneous pattern of magnetic flux density while at least one of avoiding substantial degradation

of, maintaining and improving signal-to-noise ratio performance, said method comprising the steps of:

(a) providing a model of a conventional resonator, said conventional resonator having a

first end ring and a second end ring interconnected by a plurality of rods;

(b) ascertaining said magnetic flux density within said resonator; and

(c) adjusting a geometry of at least one of said first end ring, said second end ring and said

rods, to improve the homogeneity of said magnetic flux density and thereby form said coil.

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38. (Withdrawn) The method as claimed in claim 37 wherein said coil is a birdcage coil.

39. (Withdrawn) The method as claimed in claim 37 wherein the step of providing a

model of a conventional resonator comprises using a wire model thereof.

40. (Withdrawn) The method as claimed in claim 37 wherein the step of ascertaining said

magnetic flux density involves at least one of Biot-Savart modeling and experimental verification.

41. (Withdrawn) The method as claimed in claim 37 wherein the step of adjusting

involves changing at least one of (i) a diameter of said first end ring, (ii) a diameter of said second end

ring and (iii) a radius of a taper of said rods by which said rods are connected to said end rings.

42. (Withdrawn) The method as claimed in claim 37 wherein the step of adjusting

optionally applies to a length of said rods when said signal-to-noise ratio performance of said coil is

less important.

43. (Withdrawn) The method as claimed in claim 37 wherein the step of adjusting is

performed iteratively.

44. (Withdrawn) The method as claimed in claim 37 further comprising the step of

adjusting a volume of said coil to improve said signal-to-noise ratio performance thereof.

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45. (Withdrawn) A birdcage coil for use with a magnetic resonance imaging (MRI) system

to form images of a region of interest during an MRI scanning procedure, said birdcage coil

comprising:

(a) a first ring at an inferior end of said birdcage coil, said first ring being electrically

conductive and having a first diameter through which said region of interest is provided access to said

birdcage coil;

(b) a second ring at a superior end of said birdcage coil, said second ring being electrically

conductive and having a second diameter smaller than said first diameter of said first ring; and

(c) a plurality of rods electrically interconnecting said first and said second rings to form

said birdcage coil therewith, each of said rods having a linear portion and a tapered portion with said

linear portion being connected to said first ring and said tapered portion being connected to said

second ring, said tapered portions of said rods collectively providing said birdcage coil with a

substantially homogeneous pattern of magnetic flux density in at least one of three orthogonal

imaging planes of said birdcage coil while at least one of maintaining and improving a signal-to-noise

ratio of said birdcage coil.

46. (Amended) A coil for use with a magnetic resonance (MR) system, said coil

comprising:

[(a) a plurality of conductive members each having a linear portion and a tapered portion;]

(a) [(b)] a [said] plurality of [conductive members] conductors arranged to form a first opening

at one end having a first diameter and a second opening at an other end having a second diameter

different from said first diameter; and

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(b) [(c)] at least some of said conductors each having a linear portion and a tapered portion,

with said tapered portions of said [conductive members] conductors providing said coil with a

substantially homogeneous pattern of magnetic flux density in at least one of an XZ imaging plane

and a YZ imaging plane [three orthogonal imaging planes] of said coil.

47. (Previously Presented) The coil claimed in claim 46 wherein said coil is a birdcage

coil.

48. (Previously Presented) The coil claimed in claim 46 wherein said second diameter of

said second opening is smaller than said first diameter of said first opening.

49. (Amended) The coil claimed in claim 46 wherein said tapered portion of each of said

[conductive members] at least some of said conductors comprises at least one angled linear segmented

section.

50. (Canceled)

51. (Amended) The coil claimed in claim 46 wherein said plurality of conductors includes

a first conductive ring defining said first opening [is formed by a first conductive ring] and a second

conductive ring defining said second opening [is formed by a second conductive ring], with said linear

and said tapered portions of each of said at least some of said conductors [conductive members] being

serially connected and thus electrically interconnecting said first and said second conductive rings.

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52. (Previously Presented) The coil claimed in claim 46 wherein said first opening is

adapted for accommodating insertion of a head of a patient into said coil.

53. (Amended) The coil claimed in claim 46 wherein said [conductive members]

conductors of said coil are supported by a housing therefor.

54. (Previously Presented) The coil claimed in claim 46 wherein said first and said second

openings are circular.

55. (Previously Presented) The coil claimed in claim 46 wherein said first and said second

openings are elliptical with said first diameter being a major diameter of said first opening and said

second diameter being a major diameter of said second opening.

56. (Previously Presented) The coil claimed in claim 46 wherein said coil is a receive-only

coil.

57. (Previously Presented) The coil claimed in claim 46 wherein said coil is a

transmit/receive coil.

58. (Amended) The coil claimed in claim 46 wherein said [conductive members]

conductors contain therein a plurality of reactive electrical components.

- 59. (Previously Presented) The coil claimed in claim 46 wherein said coil is configured as one of a low pass coil, a high pass coil and a band pass coil.
- 60. (Previously Presented) The coil claimed in claim 46 wherein said coil is operable in one of a linear mode and a quadrature mode.
- 61. (Withdrawn) A coil array for use with a magnetic resonance (MR) system, said coil array comprising:
 - (a) a first coil having a plurality of conductive members such that:
 - (i) each of said conductive members has a linear portion and a tapered portion;
 - (ii) said plurality of conductive members are arranged to form a first opening having a first diameter and a second opening having a second diameter, with said second diameter being different from said first diameter; and
 - (iii) said tapered portions of said conductive members providing said first coil with a substantially homogeneous pattern of magnetic flux density in at least one of three orthogonal imaging planes of said first coil; and
- (b) at least one additional coil at least partially overlapping said first coil at an inferior end thereof to form therewith, and for operation as, said coil array.
- 62. (Amended) A coil for use with a magnetic resonance (MR) system, said coil comprising:
 - (a) a first end <u>defining a first opening</u> having a first diameter;
- (b) a second end <u>defining a second opening</u> having a second diameter different from said first diameter; and

(c) a plurality of conductive rods extending between said first and said second ends, each

of said conductive rods having a linear portion and a tapered portion with said linear portion [being

connected to] extending from said first end and said tapered portion [being connected to] extending

from said second end, said tapered portions of said conductive rods providing said coil with a

substantially homogeneous pattern of magnetic flux density in at least one of an XZ imaging plane

and a YZ imaging plane [three orthogonal imaging planes] of said coil.

63. (Previously Presented) The coil claimed in claim 62 wherein said coil is a birdcage

coil.

64.

(Previously Presented) The coil claimed in claim 62 wherein said second diameter of

said second end is smaller than said first diameter of said first end.

65. (Previously Presented) The coil claimed in claim 62 wherein said tapered portion of

each of said conductive rods comprises at least one angled linear segmented section.

66. (Canceled)

67. (Previously Presented) The coil claimed in claim 62 wherein said first end includes a

first conductive ring and said second end includes a second conductive ring, with said conductive rods

electrically interconnecting said first and said second conductive rings.

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68. (Previously Presented) The coil claimed in claim 67 wherein said first conductive ring

and said second conductive ring are each larger in diameter than a center of said coil to thereby enable

a concentration of said magnetic flux density to be produced at a region centered within said coil.

69. (Previously Presented) The coil claimed in claim 62 further comprising at least one

additional coil at least partially overlapping said coil at an inferior end thereof to form therewith, and

for operation as, a phased array.

70. (Previously Presented) The coil claimed in claim 62 wherein said first and said second

ends are circular.

71. (Previously Presented) The coil claimed in claim 62 wherein said first and said second

ends are elliptical with said first diameter being a major diameter of said first end and said second

diameter being a major diameter of said second end.

72. (Previously Presented) The coil claimed in claim 62 wherein said coil is a receive-only

coil.

(Previously Presented) The coil claimed in claim 62 wherein said coil is a

transmit/receive coil.

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74. (Previously Presented) The coil claimed in claim 67 wherein each of said conductive rods and said first and said second conductive rings contain therein a plurality of reactive electrical

components.

75. (Previously Presented) The coil claimed in claim 62 wherein said coil is configured as

one of a low pass coil, a high pass coil and a band pass coil.

76. (Previously Presented) The coil claimed in claim 62 wherein said coil is operable in

one of a linear mode and a quadrature mode.

77. (Amended) A coil for use with a magnetic resonance (MR) system, said coil

comprising:

(a) a first end <u>defining</u> a first opening having a first diameter:

(b) a second end <u>defining a second opening</u> having a second diameter; and

(c) a plurality of conductive rods extending between said first and said second ends, each

of said conductive rods having a linear portion and at each end thereof [having] a tapered portion,

said tapered portions being selected to provide said coil with a subsantially homogeneous [maximize

homogeneity] pattern of magnetic flux density in at least one of an XZ imaging plane and a YZ

imaging plane of said coil.

78. (Previously Presented) The coil claimed in claim 77 wherein said first and said second

diameters of said first and said second ends, respectively, are equal.

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79. (Previously Presented) The coil claimed in claim 77 wherein said first and said second

diameters are each larger than a diameter at a center of said coil such that said tapered portions of said

conductive rods are tapered outwardly.

80. (Previously Presented) The coil claimed in claim 77 wherein said first and said second

diameters are each smaller than a diameter at a center of said coil such that said tapered portions of

said conductive rods are tapered inwardly.

81. (Previously Presented) The coil claimed in claim 77 wherein said coil is a birdcage

coil.

(c)

82. (Withdrawn) A method of designing a coil capable of exhibiting a substantially

homogeneous pattern of magnetic flux density while at least one of avoiding substantial degradation

of, maintaining and improving signal-to-noise ratio performance, said method comprising the steps of:

(a) providing a model of a conventional resonator, said conventional resonator having a

first end and a second end between which extend a plurality of conductive rods;

(b) ascertaining said magnetic flux density within said resonator; and

adjusting a geometry of at least one of said first end, said second end, and said

conductive rods to improve the homogeneity of said magnetic flux density and thereby form said coil.

83. (Withdrawn) The method as claimed in claim 82 wherein said coil is a birdcage coil.

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84. (Withdrawn) The method as claimed in claim 82 wherein said first end includes a first

conductive ring and said second end includes a second conductive ring, with said conductive rods

electrically interconnecting said first and said second conductive rings.

85. (Withdrawn) The method as claimed in claim 82 wherein the step of providing a

model of a conventional resonator comprises using a wire model thereof.

86. (Withdrawn) The method as claimed in claim 82 wherein the step of ascertaining said

magnetic flux density involves at least one of Biot-Savart modeling and experimental verification.

87. (Withdrawn) The method as claimed in claim 82 wherein the step of adjusting

involves changing at least one of (i) a diameter of said first end, (ii) a diameter of said second end and

(iii) a radius of a taper of said conductive rods at least at one end thereof.

88. (Withdrawn) The method as claimed in claim 82 wherein the step of adjusting

optionally applies to a length of said conductive rods when said signal-to-noise ratio performance of

said coil is less important.

89. (Withdrawn) The method as claimed in claim 82 wherein the step of adjusting is

performed iteratively.

90. (Withdrawn) The method as claimed in claim 82 further comprising the step of

adjusting a volume of said coil to improve said signal-to-noise ratio performance thereof.

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91. (Withdrawn) A birdcage coil for use with a magnetic resonance (MR) system for at

least one of obtaining images of a region of interest and ascertaining the spectra of said region of

interest during an MR scanning procedure, said birdcage coil comprising:

(a) an inferior end having a first diameter through which said region of interest is provided

access to said birdcage coil;

a superior end having a second diameter smaller than said first diameter of said inferior

end; and

(b)

(c) a plurality of conductive rods extending between said inferior and said superior ends,

each of said conductive rods having a linear portion and a tapered portion with said linear portion

being connected to said inferior end and said tapered portion being connected to said superior end,

said tapered portions of said conductive rods providing said coil with a substantially homogeneous

pattern of magnetic flux density in at least one of three imaging planes of said birdcage coil while at

least one of maintaining and improving a signal-to-noise ratio of said birdcage coil.

92. (Withdrawn) The birdcage coil claimed in claim 91 wherein said inferior end includes

a first conductive ring and said superior end includes a second conductive ring, with said conductive

rods electrically interconnecting said first and said second conductive rings.

93. (Withdrawn) The birdcage coil claimed in claim 91 wherein said tapered portion of

each of said conductive rods has a radius that is selected to maximize homogeneity of said magnetic

flux density in at least one of an XZ plane and a YZ plane of said imaging planes.